## IN THE SPECIFICATION:

Page 9, please amend the paragraph beginning at lines 5 and 13 as follows:

FIG. 7 is a view FIGS. 7A, 7B and 7C are used to describe an example of settings of selection conditions of residual images stored in attenuation tables 1 through 4 for the continuous radiography of FIG. 6.

As is shown in FIG. 1, an X-ray image diagnostic apparatus comprises an X-ray source 3, such as an X-ray tube, that generates X-rays, an X-ray flat panel detector 4 placed oppositely to the X-ray source 43, a C-arm 5 that supports the X-ray source 43 and the X-ray flat panel detector 3, a leg portion 6 that holds the C-arm 5 to stand on the floor, an X-ray generation high-voltage power source 7 that is electrically connected to the X-ray source 43, an image processing portion 8 that is electrically connected to the X-ray flat panel detector 3, and an image display portion (monitor) 9 that is electrically connected to the image processing portion 8.

Page 19, please amend the paragraph beginning at line 17 as follows:

Operations of the X-ray image diagnostic apparatus of the third embodiment will now be described. When the  $2 \times 2$  read fluoroscopic mode is carried out after an exposure, the control portion—11—13 controls the multiplexer 15a in such a manner that an output from the image memory 10 is inputted to the attenuation table 11d for the  $2 \times 2$  read fluoroscopic mode. Correction means same as in the first embodiment is thus applied to an image in the  $2 \times 2$  read fluoroscopic mode. Likewise, when the  $1 \times 1$  read fluoroscopic mode is carried out, the control portion 13 controls the multiplexer 15a in such a manner that an output from the image memory 10 is inputted to the attenuation table 11c for  $1 \times 1$ . Correction means same as in the first embodiment is thus applied to an image in the  $1 \times 1$  read fluoroscopic mode. Incidentally, when the read pixel size is changed during fluoroscopy, conversion is necessary because an image recorded in the image memory 10 and a fluoroscopic

image that needs correction are of different sizes. When the 2 x 2 read fluoroscopic mode is carried out before an exposure, residual image data in the  $2 \times 2$  read fluoroscopic mode is recorded in the image memory 10. Likewise, when the  $1 \times 1$ read fluoroscopic mode is carried out, residual image data in the 1 x 1 read fluoroscopic mode is recorded in the image memory 10. Normally, fast processing is required for a fluoroscopic image, and an input to the image processing portion 8 is handled in a size of the  $2 \times 2$  read fluoroscopic mode. The image memory 10 therefore has a recording size of the  $2 \times 2$  read fluoroscopic mode, too. In this case, when the fast fluoroscopic mode is switched to the high-definition fluoroscopic mode, the  $2 \times 2$  read fluoroscopic mode is carried out before an exposure, and the  $2 \times 2$ read fluoroscopic mode is changed to the 1 x 1 fluoroscopic mode after the exposure. Of the residual image data recorded in the image memory 10, data of an image region in the  $1 \times 1$  read fluoroscopic mode is sent to the attention table 11c for the  $1 \times 1$  read fluoroscopic mode. This is because when data of the image region alone is sent, high definition is maintained and yet a rate of processing speed can be taken into account by optimizing a data volume. In this instance, a single pixel in the residual image data in the 2 × 2 read fluoroscopic mode stored in the image memory 10 is inputted to four pixels at positions corresponding to this pixel in the residual image data in the 1  $\times$  1 read fluoroscopic mode within the attenuation table-12 11c. Also, the 1  $\times$  1 read fluoroscopic mode is carried out before an exposure, and 1  $\times$  1 exposure is carried out subsequently. Further, when the 1 × 1 read fluoroscopic mode is changed to the 2 × 2 read fluoroscopic mode after this exposure, neighboring four pixels within the record-image memory 10 are averaged before being input to the attenuation table, and then outputted to the 2  $\times$  2 attenuation table 11d.

Please delete pages 32-35 in their entirety.